# Applications of Phase Contrast Imaging in Congenital Heart Disease

# Kenneth Cheung

FRCR, FHKCR, FHKAM (Radiology) Cardiac Imaging Fellow at the Hospital for Sick Children, Toronto, Ontario Associate Consultant, Department of Radiology, Hong Kong Children's Hospital

cky630a@ha.org.hk





# Conflicts of Interest

No conflicts of interest

Special thanks to Dr Shi-joon Yoo Dr Davide Marini Dr Mini Pakkal all the staff at the SickKids CDIU









Figure 1. Diagrams show that spins moving along an external magnetic field gradient acquire a difference in the phase of their rotation (right), whereas nonmoving spins do not (left). The amount of phase difference is proportional to the velocity of the moving spin.  $t =$  time,  $V =$  velocity,  $\Phi =$  phase shift.



Figure 2. Principle of phase-contrast sequences available in most clinical MR imaging units. Diagram shows that two acquisitions are performed, each one with all parameters kept constant except for the flow-sensitizing bipolar gradients. The data of the two acquisitions are subtracted. The effective flow encoding is achieved by means of the difference in the bipolar gradients of the two acquisitions. This technique eliminates all phase shifts induced by imaging gradients.  $t =$  time,  $V =$  velocity.

Lotz J, Meier C, Leppert A, Galanski M. Cardiovascular flow measurement with phase-contrast MR imaging: basic facts and implementation. Radiographics. 2002 May-Jun;22(3):651-71





# What phase contrast images look like



### Phase image Magnitude image





# Paediatric considerations in CMR

- 1. Complex malformations and post-operative changes
- 2. Typical and atypical shunts
- 3. High and turbulent flows





# Technical details

Retrospective ECG gating with free breathing 25-30 phases Velocity encoding: Arteries: 150-200 cm/s, veins: 100-120 cm/s





# Applications of phase contrast imaging





# Information provided from phase contrast imaging

- 1. Flow volumes
- 2. Flow pattern
- 3. Direction of flow
- 4. (velocity)





# Applications

- 1. Assessment of flow direction
- 2. Assessment of regurgitant fraction
- 3. Assessment of shunt volume
- 4. Assessment of pulmonary blood flow for calculation of pulmonary vascular resistance
- 5. Assessment of aortopulmonary collateral flow





# 1. Assessment of flow direction



Monvadi B et al. Cardiovascular Applications of Phase-Contrast MRI. American Journal of Roentgenology 2009 192:3, 662-675





# 2. Assessment of regurgitant fraction

#### 4.3.5. Tetralogy of Fallot

#### **Recommendations for TOF** Referenced studies that support recommendations are summarized in Online Data Supplement 43, (See Section 4.3.6, for recommendations regarding evaluation and management of right ventricle-to-PA conduits.)  $COR$ **IOF Recommendations** Diagnostic 1. CMR is useful to quantify ventricular size and function, pulmonary valve function,  $B-NR$ pulmonary artery anatomy, and left heart abnormalities in patients with repaired TOE 54.3.5-1 2. Coronary artery compression testing is indicated before right ventricle-to-PA **B-NR** conduit stenting or transcatheter valve placement in repaired TOF<sup>5435-2</sup> 3. Programmed ventricular stimulation can be **Ila B-NR** useful to risk-stratify adults with TOF and additional risk factors for SCD. 54.3.5-3-54.3.5-8 4. In patients with repaired TOF, cardiac catheterization with angiography. if indicated, is reasonable to assess hemodynamics when adequate data cannot lla  $C-EO$ be obtained noninvasively in the setting of an arrhythmia, HF, unexplained ventricular dysfunction, suspected pulmonary hypertension or cyanosis.



**SALTOFICAL** 

2018 AHA/ACC Guideline for the Management of Adults With Congenital Heart Disease: A Report of the American College of Cardiology/American Heart Association Task Force on Clinical Practice Guidelines



















# 2. Estimation of regurgitant fraction

1. Pulmonary regurgitation: Backward flow/Forward flow

- 2. Aortic regurgitation: (AOV forward flow Qp)/ AOV forward flow
- 3. Tricuspid regurgitation: RVCI-MPAf/ (RVCI -MPAf) + Qs
- 4. Mitral regurgitation: LVCI AAOf/ (LVCI AAOf) + Qp

Local practice, no established consensus

 $\frac{1}{1}$ 



# 3. Assessment of shunt volume

# Qp/Qs (pulmonary blood flow/systemic blood flow)







### $Qs = QAAO$







### $Qs =$

 $\overline{\text{QSVC}}$  ( all the venous return from the upper body)

+ QDAO (all the systemic supply to the lower body)

(more reliable than direct measurement of AAO due to presence of turbulent flow)







# Qpa = Qmpa







# Qpa = QRPA + QLPA

(more reliable than direct measurement of MPA due to turbulent flow and cardiac motion)





# Example case

- 12 year old girl with history of valve sparing repair of Tetralogy of Fallot
- Previous echocardiography showed absence of residual left to right shunting
- Follow-up cardiac MRI to assess:
	- Ventricular volumes and function
	- Pulmonary regurgitation











### $Qp = Q(RPA+LPA)$

RPA 3.2 L/min/m2 LPA 2.8 L/min/m2

 $Qp = 6$  L/min/m2



# SVC= 1.4 L/min/m2  $DAO = 2.5$  L/min/m2

### $Qs = 3.9$  L/min/m2

 $Qp / Qs = 1.6$ 









# Retrospective analysis of all the follow up echocardiograms







# Retrospective analysis of all the follow up echocardiograms





# 4. Assessment of pulmonary blood flow for calculation of pulmonary vascular resistance

# Fick Principle

# **Thermodilution**



https://www.pcipedia.org/





# Limitations of the Fick principle

The Fick principle requires measurement of

- Haemoglobin
- aortic and pulmonary artery oxygen saturations and partial pressures
- oxygen consumption.

Accumulation of errors due to multiple individual measurement errors

Reduced accuracy in patients with large intra-cardiac shunts and high pulmonary blood flow





# **Thermodilution**



Teboul JL, Saugel B, Cecconi M, De Backer D, Hofer CK, Monnet X, Perel A,Pinsky MR, Reuter DA, Rhodes A, Squara P, Vincent JL, Scheeren TW. Less invasive hemodynamic monitoring in critically ill patients. Intensive Care Med. 2016 Sep;42(9):1350-9.





# Use of CMR

1. Direct measurement of pulmonary blood flow

- a. QRPA + QLPA
- b. Q (RUPV + RLPV + LUPV + LLPV) in cases of turbulence
- 2. Catheter pressure measurement



Muthurangu V et al. Novel method of quantifying pulmonary vascular resistance by use of simultaneous invasive pressure monitoring and phase-contrast magnetic resonance flow. Circulation. 2004; 110:826-834.





# 5. Assessment of aortopulmonary collateral flow



Grosse-Wortmann L, Al-Otay A, Yoo SJ. Aortopulmonary collaterals after bidirectional cavopulmonary connection or Fontan completion: Quantification with magnetic resonance





# Perioperative management of APCs prior to Fontan completion

The aortopulmonary collateral flow (relative to the cardiac index) correlated with

- the duration of hospital stay  $(P = .02)$
- and pleural drainage  $(P = .03)$ .

Grosse-Wortmann, Lars et al. Aortopulmonary collateral flow volume affects early postoperative outcome after Fontan completion: A multimodality study. The Journal of Thoracic and Cardiovascular Surgery , Volume 144 , Issue 6 , 1329 - 1336







# Qpa =QRPA + QLPA

 $Qpv = QPVs$ 

QAPC = Qpv - Qpa





#### **BCPC**



#### **OBJECTIVES:**

- Pulmonary blood flow 1.
- Aortopulmonary collaterals 2.
- Ventricular function 3.

#### PROTOCOL:



- PC of large venous decompressing channels, if present Fraunungy

#### **Fontan Operation**

#### PROTOCOL:



**Fi** 

# Workflow at SickKids

- 1. MRI performed at Cardiac Diagnostic Imaging Unit
- 2. Invasive angiography performed
- 3. Flows derived from MRI
- 4. Embolisation of collaterals if presence of significant APCs (~>50%)











# Limitations of phase contrast imaging

- 1. Motion artefacts
- 2. Partial volume artefacts
- 3. Turbulence or stenotic jets







# Future directions

### 4D Flow

### Additional information on

Wall shear stress

Turbulent kinetic energy

Vortex flows

Pressure gradient



4D flow MRI. Michael Markl et al. Journal of magnetic resonance imaging : JMRI 2012





# Questions?











# Appendix













vessel (left), whereas estimates of flow are largely preserved (right). Red line indicates the true peak velocity or true flow. Green area indicates a deviation of 10% from the true peak velocity or true flow. Bottom: Surface renderings of data from velocity images obtained at different values of  $V_{\text{enc}}$  show how increasing noise may mask the true peak velocity values. (The experimental setting consisted of the following: laminar steady flow of 2.05 L/min, gadoliniumdoped saline solution, and a 1.5-cm-diameter glass tube. The real flow rate was monitored with an inductive flowmeter. The imaging parameters were kept constant while  $V_{\text{enc}}$  was varied between 57 cm/sec and 550 cm/sec.)

Lotz J et al. Cardiovascular flow measurement with phase-contrast MR imaging: basic facts and implementation. Radiographics. 2002 May-Jun;22(3):651-71











# AR=NM Archive request accepted.



 $P_1 + \frac{1}{2}\rho v_1^2 + \rho g h_1 = P_2 + \frac{1}{2}\rho v_2^2 + \rho g h_2$ Pressure Kinetic Potential Energy Energy Energy The often cited example of the per unit per unit Bernoulli Equation or "Bernoulli volume volume Effect" is the reduction in pressure Flow velocity Flow velocity J which occurs when the fluid speed v,  $\sim$  increases.  $A_2 < A_1$  $v_2 > v_1$  $P_{2}$  <  $P_{1}$ !  $P_{2}$ Increased fluid speed, P, decreased internal pressure.

Energy per unit volume before = Energy per unit volume after







Powell AJ et al. Phase-velocity cine magnetic resonance imaging measurement of pulsatile blood

flow in children and young adults: in vitro and in vivo validation. Pediatr Cardiol.





# Commonly encountered flow patterns

### 1. PAPVC

a. Simple numbers game: Qsvc above Qsvc below









Radiology

